



- Motivation: need for accurate ion beam range verification
- Method: prompt-γ imaging via Compton scattering kinematics R&D on Compton camera (with electron tracking capability)
- Design, setup and characterization of prototype detector system



### Prompt gamma emission from proton beam on biomedical sample



- key issue in hadron therapy:
  - localization of Bragg peak within patient/sample
  - → range verification of therapeutic proton (or ion) beam

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 experimental approach: imaging via prompt γ emission from nuclear reactions  irradiation of water phantom with 100 MeV protons:



Treatment beam



exploit kinematics of Compton scattering:

$$\cos\theta = 1 - m_e c^2 \left(\frac{1}{E_2} - \frac{1}{E_1}\right)$$

(i)  $\gamma$  tracking:

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- reconstruction of incompletely absorbed events
- $\rightarrow$  increased reconstruction efficiency

= 10

y (cm



Compton camera layout:



C. Lang et al., JINST 9 (2014) P01008, PhD thesis in preparation





simulations for tracker/absorber specifications and expected performance:



- d=500  $\mu$ m + electron tracking:  $\rightarrow$  improved efficiency

- $6x6 \text{ mm}^2 \rightarrow 3x3 \text{ mm}^2 \text{ pixel}$ :
- spatial resolution improves by  $\geq$ 50 %
- $\varepsilon \approx 10^{-3} 10^{-5}$  (@ 1- 5 MeV for optimum resolution)
- angular resolution  $\approx 2^{\circ} 2.5^{\circ}$  (@ 2-6 MeV)



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## <u>Compton Camera Prototype:</u> <u>Scatter/Tracker Array</u>

- Scatterer/Tracker Array:
- 6x double-sided silicon strip detectors (DSSSD)
- $\rightarrow$  active area 50 x 50 mm<sup>2</sup>
- $\rightarrow$  thickness : 500  $\mu$ m
- $\rightarrow$  128 strips on each side
- $\rightarrow$  pitch size 390  $\mu$ m







→ replacement by modern ASIC desirable: wider dynamics, trigger, more flexibility (monitor)

### S. Aldawood, PhD thesis, in preparation

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### <u>Compton Camera Prototype:</u> <u>Scatter/Tracker Array</u>





- light tight enclosure
- Faraday cage (+ ventilation, thermal control)

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## **Compton Camera Prototype**

### Absorber:

# PMT LaBr<sub>3</sub>

LaBr<sub>3</sub> crystal: 50 x 50 x 30 mm<sup>3</sup> PMT: Hamamatsu H9500 (multi-anode: 16x16):



- signal processing:
  - 256 pixel (3x3 mm<sup>2</sup>)
  - individual spectroscopy electronics channels

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- → fast amplifier + CFD (Mesytec MCFD-16, 16 ch.)
- → charge-sensitive digital converter (Mesytec, 32 ch. VME-QDC)

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• energy resolution: 
$$\langle \Delta E/E \rangle = 3.8\% @ 662 \text{ keV} (^{137}\text{Cs})$$

H. v.d. Kolff, Master thesis, TU Delft/LMU (2014)





## **High-Energy Calibration**

- Experiment at Tandetron (HZDR, Dresden/Rossendorf):
  - low energy (~1 MeV) protons
  - $E_{\gamma}$  =4.44 MeV via <sup>15</sup>N(p, $\alpha\gamma$ )<sup>12</sup>C



ightarrow validation of MC simulations

S. Aldawood, PhD thesis, in preparation





**Scatter/Tracker Array** 

- energy deposition in 6 DSSSD layers:  $E_{\gamma} = 4.4 \text{ MeV}$ 
  - from simulation: increasing yield from front- to backside layers (accumulating contributions from Compton electrons)



 $\rightarrow$  simulations verified

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### **Commissioning at Garching** MAXIMILIANS **Tandem Accelerator** UNIVERSITÄT

20 MeV protons + water phantom: prompt- $\gamma$  spectrum



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I. Castelhano, Master thesis, U Lisbon/LMU, 2014



## LaBr<sub>3</sub> detector properties: Spatial resolution

- spatial resolution:
  - collimated  $\gamma$  source (Ø 1 mm): <sup>137</sup>Cs (662 keV, ca. 100 MBq)







### data analysis:

- background correction
- gain matching/uniformity correction: electronics, PMT
  - $\rightarrow$  "k-nearest neighbour" algorithm (TU Delft)
  - $\rightarrow$  derive position information from monolithic crystal

H.T. van Dam et al., IEEE TNS 58 (2011) 2139



## <u>LaBr<sub>3</sub> detector properties:</u> <u>Spatial resolution</u>

- light amplitude distribution maps:
  - 2D scan with collimated <sup>137</sup>Cs source
  - irradiation of 16x16 pixels (3x3 mm<sup>2</sup>)



 goal: 10<sup>4</sup> maps as reference data set (0.5 mm collimation, 0.5 mm step size)  γ hit position identification via 'k-NN': (preliminary, not yet full resolution)



T. Marinšek, Master thesis, LMU, in preparation

16 S. Aldawood, PhD thesis y Multiun preparation Semiconductor Detectors for Medical Applications, Garching, 13.2.2015



•  $\gamma$ -PET technique: reconstruct triple-coincidences from  $\beta^+\gamma$  emitters





C. Lang et al., JINST 9 (2014) P01008, PhD thesis in preparation

- $\rightarrow$  prompt- $\gamma$  detection during irradiation
- $\rightarrow$  delayed photons from  $\beta^+$  ( $\gamma$ ) emitters (<sup>11,10</sup>C, <sup>15,14</sup>O, <sup>13</sup>N) during irradiation interrupts





- Compton camera prototype for prompt-gamma range monitoring:
  - prototype characterized off- and online:
    - absorber:

LaBr<sub>3</sub> with multi-anode PMT:  $\Delta E/E = 3.8\%$ ,  $\Delta t= 270$  ps spatial characterization (k-NN method) in progress

 $\rightarrow$  prerequisite of source reconstruction (MEGAlib)

- scatterer/tracker:

6x DSSSD (500 μm, 50x50 mm<sup>2</sup>, 2x128 ch.)

- online characterization: Garching ( $E_p = 20 \text{ MeV}$ ), Dresden ( $E_{\gamma} = 4.4 \text{ MeV}$ )
- verification of model simulations
- Perspective: hybrid detector system
  - prompt- $\gamma$  detection during irradiation
  - delayed photons from  $\beta^+$  ( $\gamma$ ) emitters (<sup>11,10</sup>C, <sup>15,14</sup>O, <sup>13</sup>N) during irradiation interrupts





- LMU Munich: C. Lang, S. Aldawood, I. Castelhano, H. v.d. Kolff, S. Liprandi, B. Tegetmeyer, G. Dedes, R. Lutter, J. Bortfeldt, K. Parodi
- TU Munich: L. Maier, M. Böhmer, R. Gernhäuser
- OncoRay/ HZDR, Dresden: G. Pausch, K. Römer, J. Petzoldt, F. Fiedler
- TU Delft: D.R. Schaart



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## Thank you for your attention !